RESEARCH ARTICLE

Biomaterials Research





Mn-single-atom nano-multizyme enabled NIR-II photoacoustically monitored, photothermally enhanced ROS storm for combined cancer therapy

Xiaozhe Wang^{1,2†}, Xiaofeng Ren^{3†}, Jie Yang⁴, Zican Zhao⁴, Xiaoyu Zhang^{1,2}, Fan Yang³, Zheye Zhang⁵, Peng Chen^{5*}, Liping Li^{1,3*} and Ruiping Zhang^{1*}

Abstract

Rationale To realize imaging-guided multi-modality cancer therapy with minimal side effects remains highly challenging.

Methods We devised a bioinspired hollow nitrogen-doped carbon sphere anchored with individually dispersed Mn atoms (Mn/N-HCN) via oxidation polymerization with triton micelle as a soft template, followed by carbonization and annealing. Enzyme kinetic analysis and optical properties were performed to evaluate the imaging-guided photothermally synergized nanocatalytic therapy.

Results Simultaneously mimicking several natural enzymes, namely peroxidase (POD), catalase (CAT), oxidase (OXD), and glutathione peroxidase (GPx), this nano-multizyme is able to produce highly cytotoxic hydroxyl radical (•OH) and singlet oxygen (¹O₂) without external energy input through parallel and series catalytic reactions and suppress the upregulated antioxidant (glutathione) in tumor. Furthermore, NIR-II absorbing Mn/N-HCN permits photothermal therapy (PTT), enhancement of CAT activity, and photoacoustic (PA) imaging to monitor the accumulation kinetics of the nanozyme and catalytic process in situ. Both in vitro and in vivo experiments demonstrate that near-infrared-II (NIR-II) PA-imaging guided, photothermally enhanced and synergized nanocatalytic therapy is efficient to induce apoptosis of cancerous cells and eradicate tumor tissue.

Conclusions This study not only demonstrates a new method for effective cancer diagnosis and therapy but also provides new insights into designing multi-functional nanozymes.

Keywords Single-atom nanozymes, NIR-II photoacoustic imaging, Nanocatalytic therapy, Photothermal therapy

[†]Xiaozhe Wang and Xiaofeng Ren contributed equally to this study.

*Correspondence: Peng Chen chenpeng@ntu.edu.sg Liping Li liliping_8103@163.com Ruiping Zhang zrp 7142@sxmu.edu.cn Full list of author information is available at the end of the article



© The Author(s) 2023. Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit http://creativecommons.org/licenses/by/4.0/. The Creative Commons Public Domain Dedication waiver (http://creativecommons.org/publicdomain/zero/1.0/) applies to the data made available in this article, unless otherwise stated in a credit line to the data.



Introduction

Nanozymes, a kind of nanomaterials with intrinsic catalytic activities mimicking natural enzymes [1-3], have attracted considerable interest in cancer treatment [4-6]. Nanocatalytic cancer therapy is mainly based on the ability of nanozymes to produce cytotoxic reactive oxygen species (ROS) [7-9]. Compared to the conventional treatments, it offers high effectiveness, good tumor-specificity, and low side effects [10-12]. Single-atom nanozymes (SAEs) with atomically dispersed metal active sites are the most recent appealing addition to the nanozyme family because of their superior catalytic activity, highest atomic utilization, and highly tunable catalytic properties by engineering the coordination environment [13–18]. Current SAEs, however, usually lack sustainable catalytic activity, multi-enzymatic properties, and the ability to self-reveal their tumor accumulation and activity. And their effectiveness is often compromised by the upgraded antioxidant defense systems in tumor tissues [19-24]. Moreover, the readily fabrication of a biocompatible supporting material that ensures atomic dispersion, stable anchoring, and high loading of metal active sites is challenging.

Manganese (Mn) is a common co-factor of various metalloenzymes in humans [25–28]. This has recently spurred a curiosity to develop Mn-based SAEs. Li et al. reported a Mn-SAE that mimics peroxidase (POD) to catalyze H_2O_2 into hydroxyl radicals (•OH) [29]. The efficiency of this single-enzyme-mimicking agent is largely compromised by the limited supply of H_2O_2 in tumor tissues. Liu's group demonstrated another

Mn-SAE that simultaneously mimics POD, catalase (CAT) to catalyze H_2O_2 into O_2 , and oxidase (OXD) to convert O_2 to superoxide radicals ($\bullet O_2^-$) [30]. The potency of this multi-enzyme-mimicking agent is enhanced by parallel and cascaded catalytic reactions using multiple substrates. But it is undermined by overexpressed superoxide dismutase (SOD) in tumor tissues, which eliminates $\bullet O_2^-$. Furthermore, ROS produced by both Mn-SAEs are greatly neutralized by the overexpressed antioxidants (particularly, glutathione) in tumor tissues.

Herein, we readily fabricated a Mn-SAE by soft-templated polymerization and carbonization. With individual Mn atoms anchored by doped nitrogen atoms (Mn-N₄) populated on a hollow carbon nanosphere (Mn/N-HCN), this Mn-SAE simultaneously mimics POD, CAT, and OXD to produce $\cdot O_2^{-}$ and highly cytotoxic •OH. Furthermore, it catalyzes $\bullet O_2^-$ into more cytotoxic singlet oxygen $({}^{1}O_{2})$, and acts as glutathione peroxidase (GPx) to eliminate GSH thereby ensuring sustainable actions by the produced ROS. In addition, with wide-spectrum adsorption, Mn/N-HCN allows NIR-II photoacoustic (PA) imaging, NIR-II photothermal therapy, and significant enhancement of the CAT-mimicking activity. Monitoring the biodistribution, accumulation kinetics in tumor tissue, and in situ catalytic activity of the nanozyme by PA imaging permits the guidance and optimization of the treatment. As shown by both in vitro and in vivo experiments, the herein demonstrated NIR-II PA-imaging guided, photothermally enhanced and synergized nanocatalytic



Scheme 1. Schematic comparison between common single-atom-nanozymes (SAEs) and Mn-SAE in this work

therapy (Scheme 1) is highly efficient to induce apoptosis of cancerous cells and eradicate tumor tissue.

Methods and materials

Chemicals and agents

All the chemical reagents were analytical grade without further purification. Aniline, pyrrole, and ammonium persulphate were purchased from Energy Chemical (Anhui, China). 5,5'-Dithiobis(2- nitrobenzoic acid) (DTNB) was purchased from TCI (Shanghai, China). The superoxide anion assay kit was acquired from Suzhou Comin Biotechnology (Jiangsu, China). The H₂O₂ test kit was obtained from Nanjing Jiancheng Bioengineering Institute (Nanjing, China). The Cell Counting Kit-8 (CCK-8) kit was purchased from Sevenbio (Beijing, China). Triton X-100, calcein acetoxymethyl ester (Calcein-AM)/propidium iodide (PI) double stain kit, Annexin V-FITC Apoptosis Detection Kit, JC-1 staining kit, Acridine Orange (AO) staining kit, and 2'7'-Dichloroflfluorescein diacetate (DCFH-DA) were purchased from Beijing Solarbio Science & Technology Co., Ltd. (Beijing, China). BALB/c mice (6 weeks) were obtained from Beijing Vital River Laboratory Animal Technology Co., Ltd. VEVO LAZR instrument from FUJIFILM VisualSonics (Amsterdam, NL) operating with an LZ250 transducer was utilized for US and PA imaging.

Characterization

Transmission electron microscopy (TEM) images, elemental mapping, and energy dispersive spectrum (EDS) analysis were observed using a JEM-2100F microscope (JEOL, Japan). The zeta potential analysis and dynamic light scattering (DLS) of the nanozyme were performed on a Nano-Zetasizer (Malvern, Zetasizer Nano ZS90). A UV-Vis-NIR spectrometer (HL-2000, TS OPTICS) was used to record the absorption spectra of nanozyme. Fourier-transform infrared (FT-IR) spectra were measured by a Vertex Perkin-Elmer 580BIR spectrophotometer (Bruker) with KBr powder as the background correction to analyze the enzyme's chemical bonds and functional groups. Thermal images were obtained using a Fluke Ti400. Thermo Scientific K-alpha instrument carried out x-ray photoelectron spectroscopy (XPS) spectra to analyze the elemental composition and the valence of the Mn component of Mn/N-HCN nanozymes. An inductively coupled plasma optical emission spectrometry (ICP-OES) (PerkinElmer 8300) was conducted for quantitative analysis of the contents of elements. X-ray absorption of fine structures (XAFS) measurements of Mn K-edge are carried out at the XAS station (BL14W1) of the Shanghai Synchrotron Radiation Facility (SSRF). The electron storage ring was operated at 3.5 GeV. Si(311) doublecrystal was used as the monochromator, and the data was collected using a solid-state detector under ambient conditions. The beam size was limited by the horizontal and vertical slits with an area of 1×4 mm² during XAS measurements.

Synthesis of Mn/N-HCN

0.06 g of Triton X-100 was added to 60 mL of deionized water and mixed well, then 0.38 mL of aniline and 0.29 mL of pyrrole were added to form a homogeneous solution. Pre-cooled aqueous ammonium persulfate solution was added to the above pre-cooled homogeneous solution for polymerization for 12 h at 0 °C. The product was washed with deionized water until the filtrate was colorless, and the resulting product was dried at 60 °C in a drying oven to obtain the black powder. The drying powder was placed in a tube furnace and heated to 1000 °C under N₂ flow with a heating rate of 10 °C/min for 2 h to obtain hollow carbon nanospheres (N-HCN). 50 mg N-HCN powder was dispersed in 5 mL of deionized water by ultrasonication for 5 min. After forming a homogeneous mixture, aqueous $MnCl_2 \cdot 4H_2O$ solution was slowly dropped into the above-mixed solution under stirring at room temperature for 3 h. The product was centrifuged, washed 3 times with deionized water, and dried in the oven at 60 °C for 24 h. The obtained powder was placed in a tube furnace and heated to 1000 °C with a heating rate of 10 °C/min for another 2 h under an N₂ atmosphere to obtain the product Mn/N-HCN finally.

Measurement of peroxidase-mimic activity (POD-mimic)

The POD-mimic activity of Mn/N-HCN was measured by using 3,5,3,5'-tetramethylbenzidine (TMB) as a probe. Specifically, H_2O_2 (25 mM) was mixed with HAc-NaAc buffer, followed by the addition of Mn/N-HCN or N-HCN (100 µg/mL and TMB (0.5 mM). The absorbance at 652 nm was recorded using a UV–Vis spectrophotometer.

The concentration dependence of the POD-mimic activity of Mn/N-HCN was assessed by adding various concentrations of Mn/N-HCN (0, 12.5, 25, 50, 100 μ g/mL), H₂O₂ (25 mM) and TMB (0.5 mM) into HAc-NaAc buffer (pH=4.6), the mixture was incubated for 10 min. Finally, the absorbance at 652 nm of the mixture was detected by a UV–Vis spectrophotometer.

The kinetic assays of Mn/N-HCN with H_2O_2 as the substrate was conducted by adding TMB (0.5 mM) and various concentrations of H_2O_2 solution (0, 5, 10, 20, 40, 60, 80 mM). The absorbance of productions was monitored at different reaction times.

Measurement of catalase-like activity (CAT-mimic)

The CAT-like activity of Mn/N-HCN was detected by measuring the O_2 production through a dissolved oxygen meter. Mn/N-HCN or N-HCN (100 µg/mL) were added into -PBS (pH 4.6 or 6.2 or 7.4) containing H₂O₂ (0.5 mM). The generation of O₂ was measured at different time points. A similar method was used to detect the O₂ production of Mn/N-HCN at 25 °C and 40 °C.

Measurement of oxidase-like activity (OXD-mimic)

Superoxide Anion Assay Kit was used to detect $\cdot O_2^{-}$. The detection was performed according to the kit steps and the concentration of Mn/N-HCN was 0, 12.5, 25, 50 and 100 µg/mL.

Measurement of single oxygen $(.^{1}O_{2})$

The ability of ${}^{1}O_{2}$ generation by Mn/N-HCN was evaluated by a specific probe ABDA. ABDA can react with ${}^{1}O_{2}$ to produce endoperoxide, which will cause the fluorescence intensity decrease of ABDA. Briefly, H_2O_2 (1 mM), ABDA (1 mg/mL), and Mn/N-HCN (100 µg/mL) with or without $\cdot O_2^-$ scavenger SOD (200 units/mL) were added to the buffer (pH=6.2). Then, the changes in fluorescence intensity were detected by a fluorescence spectrophotometer after different reaction times (0, 1, 3,5, 10, 15 min).

Electron paramagnetic resonance (ESR) detects the reactive oxygen species

DMPO was used as the •OH and $\cdot O_2^-$ trapping agent for the ESR assay, and TEMP was used as the ${}^{1}O_2$ trapping agent. DMPO was mixed with Mn/N-HCN (100 µg/mL) and H₂O₂ (100 mM) in HAc-NaAc buffer (pH=4.6) to detect •OH. DMPO was mixed with Mn/N-HCN (100 µg/mL) in methanol to detect $\cdot O_2^-$. TEMP was mixed with Mn/N-HCN (100 µg/mL) and H₂O₂ (100 mM) in PBS (pH=6.2) to detect ${}^{1}O_2$. For comparison, all the groups with irradiation (1064 nm, 1.0 W/cm², 5 min) were at the same condition.

GSH depletion with Mn/N-HCN nanozymes

Mn/N-HCN (0, 50, 100, 150, 200 μ g/mL) were mixed with GSH (2 mM) in PBS, then added DTNB (0.2 mM) to detect the -SH group in GSH. A UV–Vis spectrophotometer recorded the absorbance changes after a certain reaction time. The ability of Mn/N-HCN (100 μ g/mL) to deplete GSH at appointed times was assessed using a similar method.

In vitro photothermal performance evaluation

The photothermal characteristics of Mn/N-HCN with different concentrations (0, 25, 50, 100, and 200 μ g/mL) under NIR-II laser irradiation (1064 nm, 1 W/cm²) were recorded using a thermal detector. The photothermal stability of Mn/N-HCN was evaluated by exposing it to a 1064 nm laser for 10 min, and the 1064 nm laser on/ off repetition was carried out for 5 times. The photothermal conversion efficiency (η) was calculated as follows equation.

$$\eta = \frac{hS(T_{max} - T_{surr}) - Q_{dis}}{I(1 - 10^{-A_{1064}})}$$

where S (cm²) refers to the surface area of the container; h (W cm⁻² K⁻¹) is the heat transfer coefficient; T_{max} (K) is the equilibrium temperature; T_{surr} is the surrounding ambient temperature; Q_{dis} (W) represents the heat loss due to absorption by the container which is negligible; I (W/cm²) is power intensity of the incident laser. A_{1064} means the absorbance of the Mn/N-HCN at 1064 nm. In addition, hS is calculated using the following equation:

$$hS = \frac{m_D C_D}{\tau_S}$$

where τ_s represents the time constant of the sample system; m_D and C_D are the mass and heat capacity (4.2 J g⁻¹ °C⁻¹) of DI water. τ_s is calculated using the following equations:

$$\tau_S = -\frac{\ln\theta}{t}$$
$$\theta = \frac{T - T_{surr}}{T_{max} - T_{surr}}$$

where t is irradiation time; θ means the driving force temperature.

Cell culture

The murine breast cancer line (4T1 cells) was cultured in 1640 medium containing 10% FBS and 1% penicillin–streptomycin at 37 °C under 5% CO_2 .

Cell uptake

4T1 cells were seeded in 24-well plates and incubated for 24 h. After replacing the medium with the FITC labeled Mn/N-HCN (50 μ g/mL), cells were further incubated at different times (0 h, 2 h, 4 h, 8 h, 12 h). The fluorescence imaging of cells was recorded by confocal microscopy.

Cytotoxicity assessments

4T1 cells were seeded in 96-well plates and incubated for 24 h. The different concentrations (0, 3.12, 6.25, 12.5, 25, 50, 100 μ g/mL) of Mn/N-HCN with fresh 1640 medium were added to the 96-well plate. After 10 h of incubating, the cells were irradiated with or without a 1064 nm laser (1 W/cm²) for 5 min. The cells were further incubated for another 2 h. The CCK-8 assay was used to detect cell viability.

Evaluation of cell apoptosis

For analysis of cell apoptosis, Annexin V-FITC, and PI assay were employed.4T1 cells were seeded in 96-well plates and incubated for 24 h before treatment. After that, the 1640 medium was replaced with fresh acidified 1640 containing H_2O_2 (100 μ M), Mn/N-HCN (50 μ g/mL), Mn/N-HCN (50 μ g/mL) with H_2O_2 (100 μ M) for 10 h incubation. The cells treated with Mn/N-HCN with H_2O_2 were divided into two groups, one of which was exposed to 1064 nm laser irradiation (1 W/cm²) for 5 min. After another 2 h, the cells were treated according

to the manufacturer's protocol of the apoptosis kit. Flow cytometry was employed to quantify apoptosis.

Live/dead cell staining assay

For live/dead cell staining assay, 4T1 cells were seeded in 96-well plates and incubated for 24 h before treatment. Then, the 1640 medium was replaced with fresh acidified 1640 medium containing H_2O_2 (100 μ M), Mn/N-HCN (50 μ g/mL), Mn/N-HCN (50 μ g/mL) with H_2O_2 (100 μ M) and incubated for another 10 h. The cells treated with Mn/N-HCN with H_2O_2 were divided into two groups, one of which was irradiated with a 1064 nm laser (1 W/ cm²) for 5 min. After another 2 h of incubation, the cells were washed with PBS three times, followed by staining with Calcein-AM and PI for 20 min. The cells were imaged by fluorescence microscopy.

Evaluation of intracellular O₂ generation

Intracellular oxygen production was detected using $[Ru(dpp)_3]Cl_2$ as a probe. 4T1 cells were inoculated in 96-well plates and incubated with 1640 medium for 24 h. Subsequently, the cells were incubated with 1640 medium containing 30 μ M $[Ru(dpp)_3]Cl_2$ for 12 h. After that, the cells were washed with PBS three times and further incubated with 50 μ g/mL Mn/N-HCN and 100 μ M H₂O₂ for 30 min. The cells of the laser group were exposed to a 1064 nm laser irradiation (1 W/cm²) for 5 min. After washing with PBS for three times, the cells were imaged immediately by a fluorescence microscope.

Detection of ROS in cells

ROS generation in cells was measured by using the Reactive Oxygen Species Assay Kit. 4T1 cells were seeded in 96-well plates and cultured with 1640 medium for 24 h. Then, acidified 1640 medium containing 50 μ g/mL Mn/N-HCN (with or without 100 μ M H₂O₂) was co-cultured with 4T1 cells for 12 h. After 10 h incubation, the cells of the laser group were exposed to a 1064 nm laser irradiation (1 W/cm²) for 5 min and incubated for another 2 h. Then the medium was removed, and the 1640 medium containing DCFH-DA (10 μ M) was added for 15 min. After washing with PBS for three times, the cells were imaged by a fluorescence microscope.

Analysis of lysosomal disruption

Acridine orange (AO) was used as an indicator to evaluate Mn/N-HCN-induced lysosomal damage. Briefly, 4T1 cells were seeded in 96-well plates and incubated for 24 h before treatment. After that, the 1640 medium was replaced with fresh acidified 1640 containing H_2O_2 (100 μ M), Mn/N-HCN (50 μ g/mL), Mn/N-HCN (50 μ g/mL) with H_2O_2 (100 μ M) and incubated for another 10 h. The cells treated with Mn/N-HCN with H_2O_2 were

divided into two groups, one of which was exposed to a 1064 nm laser irradiation (1 W/cm²) for 5 min. After another 2 h, the cells were washed with PBS for three times and stained with AO (10 μ M) for 20 min. The fluorescence imaging of cells was analyzed by fluorescence microscopy.

Analysis of the change of mitochondrial membrane potential

Mitochondrial membrane potential was measured by the JC-1 kit. JC-1 is a fluorescent probe that could target mitochondria. The red fluorescence indicates healthy mitochondria, while the green fluorescence indicates disrupted mitochondria. 4T1 cells were seeded in 96-well plates and incubated for 24 h. After that, the 1640 medium was replaced with fresh acidified 1640 containing H₂O₂ (100 µM), Mn/N-HCN (50 µg/mL), Mn/N-HCN (50 μ g/mL) with H₂O₂ (100 μ M) and incubated for another 10 h. The cells treated with Mn/N-HCN with H_2O_2 were divided into two groups, one exposed to a 1064 nm laser irradiation (1 W/cm²) for 5 min. After another 2 h, the cells were washed with PBS three times and treated with a JC-1 kit according to the manufacturer's protocol. The fluorescence imaging of cells was analyzed by fluorescence microscopy.

Western blot analysis

For western blots of Caspase-3, Bax, Bcl-2, and β -actin expressions, the cells were treated with the same methods. After incubation for 12 h, cells were harvested and lysed in RIPA lysis buffer. The total protein was obtained by centrifugation (11,000 rpm, 10 min). Then, the protein amounts were determined by using a bicinchoninic acid (BCA) protein assay kit according to the manufacturer's instructions. The proteins were detected for a standard western blot process.

In vivo PA imaging

PA imaging was used to monitor the injected Mn/N-HCN and the saturated vascular O_2 (s O_2) in the tumor site for 24 h. When the tumor volume reached 100 mm³, the mice were intravenously injected with Mn/N-HCN, and PA imaging was performed with a VEVO LAZR Imaging System at indicated time points (2 h, 4 h, 6 h, 8 h, 12 h, 24 h) after post-injection. 1064 nm laser irradiation (1 W/cm², 10 min) enhanced catalytic performance of Mn/N-HCN in vivo was monitored by direct intratumoral injection of Mn/N-HCN (1 mg/mL, 50µL).

In vivo antitumor assay

All animal experiments were approved by the Animal Ethics Committee of Shanxi Medical University. Female BALB/c mice were purchased from Beijing Vital River Laboratory Animal Technology Co., Ltd. The xenograft 4T1 murine breast tumor models were established through subcutaneous injection of 60 µL of 4T1 cells (1×10^{6}) in the subcutaneous mice. The tumor-bearing mice were used for anti-tumor treatment until the tumor volume reached about 100 mm³. Tumor volume = (tumor length) \times (tumor width)²/2. 4T1 tumor-bearing mice were randomly divided into four groups for the treatment of I: Control (no treatment), II: intravenous injection of PBS (200 μ L) + Laser irradiation (1064 nm; 1 W/cm²), III: intravenous injection of Mn/N-HCN (1 mg/mL, 200 µL), IV: Intravenous injection of Mn/N-HCN+Laser irradiation. Two laser irradiation groups were irradiated for 10 min. The real-time temperature changes and infrared thermal imaging images of the mice were recorded with a thermal infrared camera. The tumor size and weight were measured and recorded by a ruler and electronic balance every day. After 14 days, the mice were euthanized, and their tumor tissues were collected and weighed. The major organs (heart, lung, liver, spleen, and kidney) and tumors were collected for H&E and TUNEL staining for further histological analysis.

Statistical analysis

The experimental data were expressed quantitatively as mean \pm standard error of the mean using Student's t-test for comparison. Differences were considered statistically significant at p < 0.01 (**), p < 0.001 (***), and p > 0.05 (No significance, NS). Each experiment included at least three replicates. The GraphPad Prism 8 software was used for graph plotting.

Results and discussion

Fabrication and characterization of Mn/N-HCN

The synthesis of Mn/N-HCN is illustrated in Fig. 1A. Firstly, nitrogen-doping hollow carbon nanospheres (N-HCN) were synthesized by the formation of poly (aniline-co-pyrrole) copolymer via oxidation polymerization with triton micelle as a soft template and subsequent carbonization (Fig. S1). Then, Mn^{2+} ions were absorbed into the highly porous N-HCN, followed by annealing to generate nanospheres decorated with individually anchored Mn atoms (Mn/N-HCN). As revealed by transmission electron microscopy (TEM) and scanning electron microscope (SEM), Mn/N-HCN display hollow spherical morphology with an average diameter of 113 nm $(\pm 11.4 \text{ nm}, n=50)$ (Fig. 1B and S2). Such size is desirable for nanoparticles preferentially retained in tumor tissues through the enhanced permeability and retention (EPR) effect [31, 32]. The dynamic light scattering (DLS) analysis (Fig. S3) demonstrates that Mn/N-HCN exhibits excellent dispersibility and stability. Anchoring of Mn²⁺ was evidenced by the increase of zeta potential



Fig. 1 Characterizations of Mn/N-HCN. A Schematic illustration for the synthesis of Mn/N-HCN. B TEM image. C Energy dispersive X-ray spectroscopy elemental mapping. D High-magnification HAADF-STEM image where the bright dots corresponding to individual Mn atoms are highlighted by red circles. E XRD patterns of N-HCN and Mn/N-HCN. F-G High-resolution N 1 s and Mn 2p XPS spectra of Mn/N-HCN. H-I XANES and EXAFS spectra at the Mn K-edge. J EXAFS fitting curve in R space

of the nanoparticles from -12.97 mV to -10.6 mV (Fig. S4). The Mn content in Mn/N-HCN was quantified to be 0.75 wt% by inductively coupled plasma optical emission spectrometry (ICP-OES). Elemental mapping indicates a uniform distribution of C, N, and Mn elements (Fig. 1C). Further, individual dispersion of Mn atoms was confirmed by high-angle annular dark-field scanning transmission electron microscopy (HAADF-STEM) (Fig. 1D).

X-ray diffraction (XRD) spectrum of Mn/N-HCN exhibits two broad peaks near 22° and 43°, corresponding to graphitic carbon (Fig. 1E) [33]. It is similar to N-HCN, suggesting the absence of Mn chlorides or oxides or aggregation. X-ray photoelectron spectroscopy (XPS) survey of Mn/N-HCN also testifies the presence of Mn, N, C, and O elements (Fig. S5). The high-resolution XPS N 1 s spectrum (Fig. 1F) indicates the coexistence of pyridinic N (398.2 eV), Mn-N (399.8 eV), pyrrolic N (400.3 eV), and graphitic N (401.6 eV), suggesting that Mn is coordinated by N dopants in the graphitic carbon framework [34]. According to the high-resolution XPS Mn 2p spectrum, Mn mainly exists in the forms of Mn^{2+} (640.8 eV) and Mn^{3+} (642.2 eV) (Fig. 1G) [35]. To further determine the electronic structures and local coordination environments of Mn atoms, X-ray absorption nearedge structure (XANES) and extended X-ray absorption fine structure (EXAFS) spectroscopy at the Mn K-edge were carried out. XANES spectra in Fig. 1H show that the absorption edge of Mn K-edge is located between that of



Fig. 2 In vitro characterizations of the catalytic performance of Mn/N-HCN. **A** TMB assay for POD-mimic activity at different concentrations of Mn/N-HCN. **B** O_2 generation from the decomposition of H_2O_2 (0.5 mM) due to CAT-mimic activity of N-HCN and Mn/N-HCN. **C** The $\cdot O_2^-$ assay kit detects $\cdot O_2^-$ production of Mn/N-HCN. The increased absorption peak at 530 nm confirms the production of $\cdot O_2^-$. **D** ABDA assay for $^{1}O_2$ generation by Mn/N-HCN. **E** ESR spectra of $^{1}O_2$ at different conditions where L refers to laser irradiation and H_2O_2 concentration is 100 mM (The g value of Mn/N-HCN: **g** = 2.00665, Mn/N-HCN + H_2O_2 : **g** = 2.00665, Mn/N-HCN + H_2O_2 : **g** = 2.00666, Mn/N-HCN + H_2O_2 : **g** = 2.00665, Mn/N-HCN + H_2O_2 : **g** = 2.00666, Mn/N-HCN + H_2O_2 : **g** = 2.00665, Mn/N-HCN + H_2O_2 : **g** = 2.00666, Mn/N-HCN + H_2O_2 : **g** = 2.00665, Mn/N-HCN + H_2O_2 : **g** = 2.00666, Mn/N-HCN + H_2O_2 : **g** = 2.00665, Mn/

Mn foil and Mn_2O_3 , implying that the oxidation state of Mn species lies between 0 and +3, consistent with XPS analysis [36]. As shown by Fourier transformed (FT) κ^3 -weighted EXAFS (Fig. 1I), Mn/N-HCN presents a major scattering peak at ~ 1.60 Å corresponding to the Mn-N bond, which is distinct to Mn–Mn peak at 2.30 Å in Mn foil, Mn–O peak at 1.47 Å in Mn₂O₃, and Mn–O peak at 1.40 Å in MnO [37, 38]. This observation confirms that Mn is atomically dispersed and coordinated by N. Least-squares fitting of EXAFS spectra (Fig. 1J; S6 and Table S1) suggest that Mn is coordinated by 4 N atoms with a bond length of 2.07 Å (Fig. S7) [39].

In vitro catalytic capacity

Mimicking POD activity, Mn/N-HCN can decompose H_2O_2 to generate highly cytotoxic •OH radical. This is testified by electron spin resonance (ESR) spectroscopy using 5,5-Dimethyl-1-pyrroline N-oxide (DMPO) as a spin trapper for •OH (Fig. S8) [40]. Using 3,3,5,5-tetramethylbenzidine (TMB) as the chromogenic substrate, which turns into blue color with strong absorption at 652 nm upon being oxidized by •OH [41], it was observed that the potency of nanozyme's POD activity was enhanced with increasing concentrations of Mn/N-HCN and H_2O_2 (Fig. 2A and S9) and decrease of pH (Fig. S10).

The acidic microenvironment in tumor tissues is favorable for tumor-specific nanocatalytic therapy. The Michaelis–Menten constant (K_m) and maximum initial velocity (V_{max}) of Mn/N-HCN (0.078 mM and 1.99×10^{-7} M s⁻¹, respectively) outperform natural horseradish peroxidase (0.434 mM and 1.0×10^{-7} M s⁻¹, respectively) (Fig. S11) [42, 43]. Moreover, Mn/N-HCN exhibits markedly higher POD activity than N-HCN, implying that the catalytic activity highly depends on Mn active centers. (Fig. S12).

Also mimicking CAT activity, Mn/N-HCN catalyzes the production of O_2 in the presence of H_2O_2 as detected by an oxygen meter, and it is much more potent than N-HCN (Fig. 2B). This reaction would only be slightly suppressed in the acidic tumor microenvironment (Fig. S13). Hypoxia in tumor tissues is unfavorable for the generation of ROS, thereby compromising the effectiveness of typical nano-catalytic therapy and conventional chemodynamic therapy. CAT activity of Mn/N-HCN alleviates this issue.

Mn/N-HCN demonstrates OXD activity as well, which catalyzes O_2 to $\bullet O_2^-$. The production of $\bullet O_2^-$ was detected by light absorption at 530 nm using a specific superoxide anion assay kit (Fig. 2C). Additionally, ESR measurements with DMPO as the spin-trapper revealed the presence of the characteristic quadruple peaks (1:1:1:1), confirming the nanozyme's OXD activity (Fig. S14) [44]. But in tumor tissues, $\bullet O_2^-$ can be largely scavenged by overexpressed SOD. Interestingly, it was found that Mn/N-HCN can produce highly cytotoxic ¹O₂ without any light exposure, as detected by the ${}^{1}O_{2}$ specific probe 9,10-anthracenediyl-bis(methylene) dimalonic acid (ABDA) (Fig. 2D). The characteristic absorption peak of ABDA decreased over time, indicating continuous production of ¹O₂. Using 2,2,6,6-tetramethylpiperidine-Noxyl (TEMP) as the spin-trapper, the generation of ${}^{1}O_{2}$ was further evidenced by the typical 1:1:1 triplet ESR signal (Fig. 2E) [45]. Usually, nanozymes can only produce $^{1}O_{2}$ upon laser, X-ray, or ultrasound irradiation [46]. In contrast, Mn/N-HCN requires no external energy input. Using SOD to scavenge $\cdot O_2^-$, the production of 1O_2 was completely inhibited (Fig. S15), suggesting that ${}^{1}O_{2}$ was resulted from a catalytic reaction cascaded from the OXD activity of Mn/N-HCN. Conversion of $\bullet O_2^-$ to 1O_2 , possibly through the Russell mechanism, has also been observed from other nanozymes [47]. In the presence of H_2O_2 , the production of 1O_2 was augmented through the cascade from CAT to OXD to Russell reaction (Fig. 2E). Taken together, Mn/N-HCN nano-multizyme can effectively catalyze H_2O_2 and O_2 existing in tumor tissues to produce highly toxic •OH and ${}^{1}O_{2}$ through both parallel and cascaded catalytic reactions. Glutathione (GSH), which is a highly expressed antioxidant in the tumor microenvironment, hampers the therapeutic efficiency of ROS-dependent cancer therapy [48]. Desirably, Mn/N-HCN is able to consume GSH, mimicking glutathione peroxidase (GPx). GSH can react with 5,5'-dithiobis (2-nitrobenzoic acid) (DTNB) to produce TNB. As shown in Fig. 2F and Fig. S16, the characteristic adsorption peak of TNB at 412 nm decreases with increasing Mn/N-HCN concentration and reaction time, suggesting the GPx activity of Mn/N-HCN.

Mn/N-HCN has strong light adsorption ranging from visible to NIR-II region (Fig. S17) and high photothermal conversion efficiency in a nanoparticle concentration and time-dependent manner (Fig. 2G). With 1064 nm laser irradiation at 1 W cm⁻², the temperature of PBS solution with 50 μ g/mL Mn/N-HCN increased from 23.7 to 61.1 °C within 8 min. The photothermal conversion efficiency was calculated to be 31.22% (Fig. S18) [49, 50]. Moreover, Mn/N-HCN exhibits good cycling photostability (Fig. S19). Interestingly, the CAT activity of the nanozyme can be immediately enhanced upon 1060 nm laser irradiation, correlating with the quick temperature increase due to the strong photothermal effects of the nanoparticles (Fig. 2H). Similarly, the nanozymes in the warm solution were more CAT-active.

Taken together, with five synergistically coupled nanocatalytic activities (POD, CAT, OXD, GPx, and Russell reaction), Mn/N-HCN is able to sustainably and effectively produce highly cytotoxic hydroxyl radical (•OH) and singlet oxygen ($^{1}O_{2}$) in the tumor microenvironment characterized by hypoxia and upregulated antioxidant defense (Fig. 2I). Additionally, its excellent photothermal property further promotes the production of $^{1}O_{2}$ and allows NIR-II photoacoustic imaging to guide and monitor nanocatalytic therapy in situ.

In vitro cellular assays

By labeling Mn/N-HCN with the green fluorescein dye Fluorescein Isothiocyanate (FITC), it was observed through confocal microscopy that the uptake of Mn/N-HCN by cells occurred in a time-dependent manner (Fig. S20). Based on cell viability tests, it was observed that Mn/N-HCN shows good biocompatibility to non-cancerous mouse fibroblast cells (L-929), but certain toxicity to mouse breast cancer cells (4T1), because H₂O₂ is more abundantly available in cancerous cells to be catalyzed into ROS by the nanozyme (Fig. S21). As expected, the addition of H₂O₂ into the culture medium and the application of laser irradiation (1064 nm) greatly enhanced the cytotoxicity. The live/dead cell staining analyses (Fig. S22) and flow cytometric measurements (Fig. S23) further confirmed the potent induction of tumor cell apoptosis by photothermally enhanced and synergized nanocatalytic therapy. Compared to the untreated control group, the Mn/N-HCN treated groups exhibited a noticeable increase in late apoptosis-induced cell



Fig. 3 Apoptosis of cancerous 4T1 cells induced by Mn/N-HCN. **A** Intracellular ROS level. Scale bars = 50 μ m. **B** AO staining. Fluorescence turns red once AO enters the cytoplasm due to compromised lysosomal integrity. Scale bars = 50 μ m. **C** JC-1 analysis. At normal depolarized mitochondrial membrane potential. JC-1 molecules aggregate and emit red fluorescence. Scale bars = 50 μ m. **D** Expression of apoptotic proteins revealed by immunoblotting, and (**E**) Statistic analysis normalized to actin expression. Note: different treatments: (I) Control, (II) H₂O₂ (100 μ M), (III) Mn/N-HCN (50 μ g/mL), (IV) Mn/N-HCN + H₂O₂, (V) Mn/N-HCN + H₂O₂ + 1064 nm laser (1 W/cm²). Statistical analysis was analyzed using Student's t-test for comparison. (**P* < 0.05, ***P* < 0.001, n.s. = not significant.)

death. The percentage of apoptotic cells in the Mn/N-HCN+H₂O₂+laser group was significantly higher than that in both the Mn/N-HCN+H₂O₂ and Mn/N-HCN groups, indicating that the efficacy of nanocatalytic therapy can be greatly enhanced by leveraging the photothermal effect and H₂O₂ abundance in the tumor microenvironment.

The intracellular ROS level was monitored by 2,7-dichlorofluorescein diacetate (DCFH-DA), which can be oxidized by ROS to produce green fluorescent DCF. As shown in Fig. 3A, Mn/N-HCN+ H_2O_2 +laser treatment gave the strongest fluorescence compared to the other treatments, suggesting enhanced ROS production due to increased O_2 availability resulting from the photothermally enhanced CAT activity of

Mn/N-HCN. Indeed, it was confirmed that the intracellular O_2 was highest with Mn/N-HCN+H₂O₂+laser treatment, using [Ru(dpp)₃]Cl₂ as the probe whose fluorescence is quenched by O₂ (Fig. S24).

Furthermore, using acridine orange (AO) as the indicator of lysosomal integrity (Fig. 3B) and 5,5;6,6'-tetrachloro-1,1;3,3'-tetraethyl-imidacarbocyanine iodide (JC-1) as the indicator of mitochondrial membrane potential (Fig. 3C), it was concluded that photothermally-enhanced nanocatalytic therapy significantly induced apoptosis of tumor cells via lysosomal and mitochondrial disruption dependent pathways. Consistently, immunoblotting of apoptotic proteins showed that Bcl-2 was down-regulated whereas caspase-3 and Bax were up-regulated (Fig. 3D and E).



Fig. 4 In vivo PA imaging. **A** Intra-tumor PA imaging of Mn/N-HCN and sO₂ level after intravenous injection of Mn/N-HCN. Scale bar = 2 mm. **B** Quantification of PA intensity and sO₂ level from (A). **C** Change of sO₂ level after intratumoral injection of Mn/N-HCN and 1064 nm laser irradiation. **D** Schematic illustration of NIR-II/I PA monitoring

In vivo PA imaging

The photothermal effect of Mn/N-HCN enables photoacoustic (PA) imaging in a wide wavelength range reaching NIR-II (Fig. S25), with the signal intensity linearly proportional to the nanozyme concentration (Fig. S26). Mn/N-HCN is highly biocompatible because it doesn't cause noticeable hemolysis even at a dose as high as 200 µg/mL (Fig. S27). Before injecting Mn/N-HCN into the tail vein, utilize Dspe-PEG-NH2 to increase the circulation time and stability. PA imaging enabled by Mn/N-HCN was then evaluated in vivo on tumor-bearing mice. As shown in Fig. 4A, the NIR-II PA signal in the tumor area became prominent 2 h after intravenous injection of Mn/N-HCN and reached the maximum at 6 h. Thereafter, NIR-II PA signals gradually decayed because of the clearance of Mn/N-HCN from tumor. This experiment demonstrates that the nanozyme preferentially accumulates in tumor tissues via the EPR effect, and 6 h after injection is the optimal treatment time (Fig. 4B). Moreover, NIR-II PA imaging revealed that nanozyme also accumulated in metabolic organs (liver, kidney, spleen) as expected but had little presence in heart and lung (Fig. S28).

Oxyhemoglobin and deoxyhemoglobin are the major endogenous NIR absorbers. Blood oxygen saturation (sO_2) can be determined based on their strong NIR-I PA signals. As O_2 is the key intermediate product in the catalytic cascade reaction of Mn/N-HCN, PA imaging of sO₂ enables non-invasive real-time monitoring of the nanocatalytic therapy. After systemic intravenous administration of Mn/N-HCN, its accumulation kinetics and change of sO₂ in tumor site are highly synchronized, demonstrating the nanozyme's ability to efficiently produce O_2 in situ (Fig. 4B). Consistently, after direct injection of Mn/N-HCN into tumor tissue, sO₂ level was immediately elevated by 47.1% because of the enzyme's CAT activity (Fig. 4C). It was further enhanced by 23.7% after NIR-II laser irradiation for 10 min, further confirming that the nanozyme's CAT activity can be photothermally enhanced in tumor environment. In sum, NIR PA imaging permits non-invasive, real-time, in situ monitoring of the biodistribution, tumor accumulation, and catalytic activity of the nanozyme, thereby providing guidance for the photothermally-enhanced nanocatalytic therapy and insights into its working mechanisms (Fig. 4D).

In vivo anti-tumor assessment

The in vivo therapeutic effects of intravenously injected Mn/N-HCN on the 4T1-bearing mice were evaluated. In the course of 2 weeks, 4 groups of mice received different treatments: I: Control (intravenous injection of 200 μ L PBS), II: intravenous injection of PBS+Laser irradiation (1064 nm; 1 W/cm²), III: intravenous injection of Mn/N-HCN (1 mg/mL, 200 μ L), IV: Intravenous injection of Mn/N-HCN+Laser irradiation. The laser was applied 6 h after injection when the Mn/N-HCN accumulation in tumor tissue reached the maximum. As



Fig. 5 In vivo photothermally enhanced and synergized nanocatalytic therapy. **A** Infrared thermography of mice. **B** Temperature increase at tumor sites of mice. **C** Tumor growth curves. **D** Tumor weights on day 14. **E** Photographs of typically harvested tumors at day 14 after the treatments. **F** TUNEL and H&E staining of tumor tissues (Scale bar = 50 μ m). In C-F), Mice were divided into 4 treatment groups as described in the main text. I: Control (intravenous injection of 200 μ L PBS), II: intravenous injection of PBS + Laser irradiation (1064 nm; 1 W/cm²), III: intravenous injection of Mn/N-HCN (1 mg/mL, 200 μ L), IV: Intravenous injection of Mn/N-HCN + Laser irradiation. (Statistical analysis was analyzed using Student's t-test for comparison. **P* < 0.05, ***P* < 0.01, ****P* < 0.001, n.s. = not significant.)

presented in Fig. 5A and B, laser irradiation (1064 nm, 1 W/cm²) raised the temperature at tumor area to 54.0 °C within 3 min, while the temperature only increased to 40.0 °C without the nanozymes. Tumor volume was measured every 2 days. For groups I and II, the tumor volume continued to increase substantially, while Mn/N-HCN treatment (group III) significantly

suppressed the tumor growth (Fig. 5C and S29). In comparison, Mn/N-HCN plus 1064 nm laser irradiation (group IV) totally inhibited tumor growth, demonstrating the high potential of photothermally enhanced nanocatalytic therapy. Finally, all mice were euthanatized, and the tumor tissues were harvested, photographed, weighed, and analyzed. The average weight of tumor tissues harvested from the mice treated with Mn/N-HCN plus 1064 nm laser is significantly lower than the other three groups (Fig. 5D and E). In comparison to the group I, the tumor growth inhibition of Mn/N-HCN treatment (group III) was 45.5%, while that of Mn/N-HCN plus 1064 nm laser treatment (group IV) was 91.5%, respectively (Fig. S30). Notably, 3 out of 5 mice in group IV achieved complete tumor elimination. The average body weights of all treated mouse groups are similar and remain steady during the treatment course, indicating that both Mn/N-HCN and laser treatment do not induce systemic toxicity (Fig. S31).

Terminal-deoxynucleotidyl transferase-mediated deoxyuridine triphosphate nick end labeling (TUNEL) immunofluorescence staining and hematoxylin and eosin (H&E) staining of the tumor tissues showed Mn/N-HCN plus laser treatment gave the most significant tumor damage with severe necrosis, nuclear condensation, and cellular atrophy (Fig. 5F). Meanwhile, no noticeable pathological abnormality was observed in major organs, such as heart, liver, spleen, lung, and kidney, indicating the long-term biosafety of Mn/N-HCN (Fig. S32). Taken together, the PA-imaging guided, photothermally enhanced and synergized nanocatalytic cancer therapy based on Mn/N-HCN nano-multizyme is safe and highly efficient.

Discussion

Given that limited intratumoral H_2O_2 level and hypoxia in the TME, the parallel catalytic therapy could take advantage of multiple reactants within the tumor, such as H_2O_2 and O_2 , and concurrently generate a variety of ROS to enhance the tumor therapeutic efficacy. However, overexpressed GSH in the TME is another bottleneck for ROS-involved therapy. Accordingly, nanocatalytic cancer therapy is developed as an efective strategy to suppress tumor growth by producing cytotoxic ROS and eliminate GSH.

In this study, we designed a nanocatalytic Mn-based nanozymes Mn-SAE simultaneously mimics POD, CAT, and OXD to produce $\cdot O_2^-$ and highly cytotoxic \cdot OH. Furthermore, it catalyzes $\cdot O_2^-$ into more cytotoxic singlet oxygen (1O_2), and acts as glutathione peroxidase (GPx) to eliminate GSH thereby ensuring sustainable actions by the produced ROS.Moreover, Mn/N-HCNs possess excellent photothermal properties, which can enhance the above-mentioned catalytic process while enable PA imaging. The time-course signals of Mn/N-HCN were strongly consistent with the sO₂ signals, demonstrating that the efficient O₂ production in tumors is mediated by the high catalytic effect of Mn/N-HCN.

In spite of the fact that we have only preliminarily evaluated the therapeutic efficacy of Mn/N-HCN and photoacoustic in situ monitoring in a tumor mouse model, our work suggests that the combination of Mn/N-HCN with photothermal therapy can significantly inhibit tumor growth, and also that Mn/N-HCN is a promising tworegion photoacoustic contrast agent. Whether it can be used in the preclinical field in the future is worth watching.

Conclusion

Inspired by the existence of many Mn-dependent enzymes in carbon-based lifeforms, we devised a nanomultizyme with Mn-N₄ catalytic centers atomically dispersed on a nitrogen-doped hollow carbon nanosphere (Mn/N-HCN), which is biocompatible and has a size desirable for preferential accumulation in tumor through EPR effect. Mn/N-HCN mimics the activities of four natural enzymes, including peroxidase (POD), catalase (CAT), oxidase (OXD), and glutathione peroxidase (GPx), and can also catalyze Russell reaction. Through parallel and in-series nanocatalytic reactions, the nano-multizyme can effectively produce highly cytotoxic ROS (•OH and ${}^{1}O_{2}$) without the need of external energy input and simultaneously deplete upregulated antioxidant GSH. In addition, owing to high absorption in deep-tissue-penetrating NIR-II light, Mn/N-HCN provides photothermal therapy to synergize with and enhance nanocatalytic chemotherapy and enables photoacoustic imaging to guide the dual-modal treatment by revealing the biodistribution kinetics and monitoring the catalytic process in situ. This study not only demonstrates a new method for effective cancer diagnosis and therapy but also provides new insights into designing multi-functional nanozymes. In the future, we will employ photothermal-enhanced nanocatalytic strategies for treating a broader range of tumor models and monitoring catalytic process in real-time, dynamically, and quantitatively using NIR-II PA imaging.

Abbreviations

POD	Peroxidase
CAT	Catalase
OXD	Oxidase
GPx	Glutathione peroxidase
GSH	Glutathione
•OH	Hydroxyl radical
¹ O ₂	Singlet oxygen
•0 ₂ ⁻	Superoxide radicals
PTT	Photothermal therapy
NIR-II	Near-Infrared-II
PA	Photoacoustic
ROS	Reactive oxygen species
SAEs	Single-atom nanozymes
SOD	Superoxide dismutase
ТМВ	3,5,3',5'-Tetramethylbenzidine
ABDA	9,10-Anthracenediyl-bis(methylene) dimalonic acid
ESR	Electron paramagnetic resonance
TEMP	2,2,6,6-Tetramethylpiperidine-N-oxyl
DMPO	5,5-Dimethyl-1-pyrroline N-oxide
DTNB	5,5'-Dithiobis 2-nitrobenzoic acid
DCFH-DA	2.7-Dichlorodi-hydrofuorescein diacetate

AO	Acridine orange
sO ₂	Saturated vascular O

H&E Hematoxylin-eosin staining

Supplementary Information

The online version contains supplementary material available at https://doi.org/10.1186/s40824-023-00464-w.

Additional file 1: Figure S1. TEM image of N-HCN. Figure S2. SEM image of Mn/N-HCN. Figure S3. The average size (A) and polydispersity index (B) of Mn/N-HCN in water at different time. Figure S4. Zeta potential of Mn/N-HCN. Figure S5. XPS spectra of Mn/N-HCN. Figure S6. PEXAFS fitting curves of (A) Mn₂O₃, (B) MnO, and (C) Mn foil in R space. Figure S7. The proposed Mn-N₄-C local environment of Mn/N-HCN. Figure S8. ESR spectra of •OH with characteristic quartet signal (1:2:2:1) of DMPO-OH. Figure S9. Time-course absorbance changes of TMB with the addition of different concentrations of H₂O₂. Figure S10. TMB assay for measuring POD-mimic activity of Mn/N-HCN from pH 4.6 to pH. Figure S11. (A) Michaelis-Menten kinetics curves for the POD-mimic activity of Mn/N-HCN, (B) corresponding Lineweaver-Burk plots. Figure S12. TMB assay for measuring POD-mimic activity of Mn/N-HCN. Figure S13. pH-dependent CAT-mimic activity of Mn/N-HCN. Figure S14. ESR spectra of •O₂⁻ with characteristic peaks 1:1:1:1 of DMPO-OOH. Figure S15. ABDA assay for ¹O₂ generation by Mn/N-HCN, in the presence of SOD. Figure S16. GSH depletion by Mn/N-HCN during different times. Figure S17. UV-Vis-NIR spectra of N-HCN and Mn/N-HCN. Figure S18. Calculation of photothermal conversion efficiency of Mn/N-HCN (100 µg/mL) under irradiation with 1064 nm laser (1 W/cm²). Red curve: Photothermal profile of Mn/N-HCN irradiated for 7 min. Blue curve: followed by nature cooling. Linear time data versus $-\ln(\theta)$ obtained from the cooling period. Figure S19. Temperature of Mn/N-HCN containing PBS solution subjecting to on/off cycling of laser irradiation. Figure S20. Uptake of FITC-label Mn/N-HCNs by 4T1 cells at different times. Figure S21. (A) Cell viability of L929 cells was detected by the CCK-8 method after 12 h-treatment of Mn/N-HCN at different concentrations. (B) Cell viability of 4T1 cells after 12 h-treatment of Mn/N-HCN at different concentrations and conditions. Figure S22. Live/dead cell assay. The green signal from Calcein-AM indicates live cells and the red signal from PI indicates dead cells. Scale bars=50 $\mu\text{m}.$ Figure S23. Flow cytometric measurement on cells co-stained with Annexin V-FITC and Pl. Figure S24. Intracellular O₂ generation using [Ru(dpp)₃] Cl₂ as a probe: (I) Control; (II) Mn/N-HCN+H₂O₂ (100 µM); (III) Mn/N-HCN+H₂O₂+L. Scale bars=50µm. Figure S25. The photoacoustic spectra of the Mn/N-HCN. The wavelength range is from 1200 nm to 1600 nm. Figure S26. (A) NIR-II (1200 nm) PA signal of Mn/N-HCN at different concentrations in PBS. (B) PA intensity to nanoparticle concentration with a linear fitting. Figure S27. In vitro haemocompatibility assay of Mn/N-HCN with different concentrations ranges from 0 to 200 µg/mL. Figure S28. Biodistribution of Mn/N-HCN in various organs after 6 h post-injection. Figure S29. Photographs of tumors at 1, 7, and 14 day after different treatments (I Control, II PBS+laser, III Mn/N-HCN, IV Mn/N-HCN+Laser). Figure S30. Tumor Inhibition Rate after different treatments (I Control, II PBS+laser, III Mn/N-HCNs, IV Mn/N-HCN+Laser). Figure S31. Body weight during 14 days (I Control, II PBS+laser, III Mn/N-HCNs, IV Mn/N-HCN+Laser). Figure S32. H&E staining of major organs (heart, liver, spleen, lung, and kidney) dissected from the BALB/c mice with different treated groups (I Control, II PBS+laser, III Mn/N-HCN, IV Mn/N-HCN+Laser) for post 14 days injection (Scale bar: 50 µm). Table S1. Parameters of EXAFS fits for Mn foil, MnO, Mn₂O₃, and Mn/N-HCN.

Acknowledgements

Xiaozhe Wang and Xiaofeng Ren contributed equally to this manuscript. All authors have given approval to the final version of the manuscript.

Authors' contributions

XW: responsible for conducting all experiments, and was a major contributor in writing the manuscript. XR: responsible for cell culture work, formal analysis, and data curation. JY: writing contribution to the original draft. ZZ: experiments for in vivo studies. XZ: supporting experiments for in vivo studies. FY: writing contribution to the original draft. ZZ: formal analysis. PC: responsible for project design and writing contribution to the original draft. LL: conceptualization, funding acquisition, supervision, writing – review & editing. RZ: project administration, project design, funding acquisition, supervision. All authors read and approved the final manuscript.

Funding

This work was financially supported by the National Nature Science Foundation of China (U22A20349, 82120108016, 82071987, and 82001962), the Central Government Guided Local Science and Technology Development Fund Research Project (YDZJSX20231A055), Research Project Supported by Shanxi Scholarship Council of China (No. 2020–177), Fund Program for the Scientific Activities of Selected Returned Overseas Professionals in Shanxi Province (NO: 20200006), Four Batches of Scientific Research Projects of Shanxi Provincial Health Commission (NO: 2020TD11, NO: 2020SYS15, 2020XM10), Key Laboratory of Nano-imaging and Drug-loaded Preparation of Shanxi Province (NO: 202104010910010), and Singapore Ministry of Education (AcRF Tier-2 grant, MOE2019-T2-2–004).

Availability of data and materials

The datasets used and/or analyzed during the current study are available from the corresponding author on reasonable request.

Declarations

Ethics approval and consent to participate

All animal experiments were conducted according to the protocols approved by the Institutional Animal Care and Use Committee of the Animal Experiment Center of Shanxi Medical University (No.2016LL141, Taiyuan, China).

Consent for publication

Not applicable.

Competing interests

The authors declare that they have no competing interests.

Author details

¹The Radiology Department of First Hospital of Shanxi Medical University, First Hospital of Shanxi Medical University, Taiyuan 030001, China. ²College of Medical Imaging, Shanxi Medical University, Taiyuan 030001, China. ³Department of Biochemistry and Molecular Biology, School of Basic Medical Sciences, Shanxi Medical University, Taiyuan 030001, China. ⁴Third Hospital of Shanxi Medical University, Shanxi Bethune Hospital, Shanxi Academy of Medical Sciences, Taiyuan 030032, China. ⁵School of Chemistry, Chemical Engineering and Biotechnology, Lee Kong Chian School of Medicine, Institute for Digital Molecular Analytics and Science, Nanyang Technological University, 62 Nanyang Drive, Singapore 637459, Singapore.

Received: 26 September 2023 Accepted: 20 November 2023 Published online: 04 December 2023

References

- Wei H, Wang E. Nanomaterials with enzyme-like characteristics (nanozymes): next-generation artificial enzymes. Chem Soc Rev. 2013;42:6060–93.
- Yang W, Yang X, Zhu L, Chu H, Li X, Xu W. Nanozymes: activity origin, catalytic mechanism, and biological application. Coord Chem Rev. 2021;448:214170.
- Huang Y, Ren J, Qu X. Nanozymes: classification, catalytic mechanisms, activity regulation, and applications. Chem Rev. 2019;119:4357–412.
- Zhang X, Chen X, Zhao Y. Nanozymes: versatile platforms for cancer diagnosis and therapy. Nanomicro Lett. 2022;14:95.
- Chen H, Zhang W, Zhu G, Xie J, Chen X. Rethinking cancer nanotheranostics. Nat Rev Mater. 2017;2:17024.
- Fu L, Wan Y, Qi C, He J, Li C, Yang C, et al. Nanocatalytic theranostics with glutathione depletion and enhanced reactive oxygen species generation for efficient cancer therapy. Adv Mater. 2021;33:2006892.

- Yang B, Ding L, Yao H, Chen Y, Shi J. A metal-organic framework (MOF) Fenton nanoagent-enabled nanocatalytic cancer therapy in synergy with autophagy inhibition. Adv Mater. 2020;32:1907152.
- Qian X, Zhang J, Gu Z, Chen Y. Nanocatalysts-augmented Fenton chemical reaction for nanocatalytic tumor therapy. Biomaterials. 2019;211:1–13.
- Cao F, Zhang Y, Sun Y, Wang Z, Zhang L, Huang Y, et al. Ultrasmall nanozymes isolated within porous carbonaceous frameworks for synergistic cancer therapy: enhanced oxidative damage and reduced energy supply. Chem Mater. 2018;30:7831–9.
- Kalyane D, Choudhary D, Polaka S, Goykar H, Karanwad T, Rajpoot K, et al. Reactive oxygen nano-generators for cancer therapy. Prog Mater Sci. 2022;130:100974.
- Gao G, Jiang Y, Guo Y, Jia H, Cheng X, Deng Y, et al. Enzyme-mediated tumor starvation and phototherapy enhance mild-temperature photothermal therapy. Adv Funct Mater. 2020;30:1909391.
- 12. Yang B, Chen Y, Shi J. Nanocatalytic medicine. Adv Mater. 2019;31:1901778.
- Fan Y, Liu S, Yi Y, Rong H, Zhang J. Catalytic nanomaterials toward atomic levels for biomedical applications: from metal clusters to single-atom catalysts. ACS Nano. 2021;15:2005–37.
- Zhu Y, Wang W, Gong P, Zhao Y, Pan Y, Zou J, et al. Enhancing catalytic activity of a nickel single atom enzyme by polynary heteroatom doping for ferroptosis-based tumor therapy. ACS Nano. 2023;17:3064–76.
- Chen Q, Zhang M, Huang H, Dong C, Dai X, Feng G, et al. Single atom-doped nanosonosensitizers for mutually optimized sono/ chemo-nanodynamic therapy of triple negative breast cancer. Adv Sci. 2023;10:2206244.
- Song Z, Zhang L, Doyle Davis K, Fu X, Luo J, Sun X. Recent advances in MOF-derived single atom catalysts for electrochemical applications. Adv Energy Mater. 2020;10:2001561.
- Muhammad P, Hanif S, Li J, Guller A, Rehman FU, Ismail M, et al. Carbon dots supported single Fe atom nanozyme for drug-resistant glioblastoma therapy by activating autophagy-lysosome pathway. Nano Today. 2022;45:101530.
- Zhu D, Chen H, Huang C, Li G, Wang X, Jiang W, et al. H₂O₂ self-producing single-atom nanozyme hydrogels as light-controlled oxidative stress amplifier for enhanced synergistic therapy by transforming "cold" tumors. Adv Funct Mater. 2022;32:2110268.
- Lu J, Jiang Z, Ren J, Zhang W, Li P, Chen Z, et al. One-pot synthesis of multifunctional carbon-based nanoparticle-supported dispersed Cu2+ disrupts redox homeostasis to enhance CDT. Angew Chem Int Ed. 2022;61:e202114373.
- 20. Asantewaa G, Harris IS. Glutathione and its precursors in cancer. Curr Opin Biotechnol. 2021;68:292–9.
- Cheng J, Li L, Jin D, Dai Y, Zhu Y, Zou J, et al. Boosting ferroptosis therapy with iridium single atom nanocatalyst in ultra-low metal content. Adv Mater. 2023;35:2210037.
- 22. Peng Y, Lu B, Chen S. Carbon-supported single atom catalysts for electrochemical energy conversion and storage. Adv Mater. 2018;30:1801995.
- Zhou Y, Tao X, Chen G, Lu R, Wang D, Chen M, et al. Multilayer stabilization for fabricating high-loading single-atom catalysts. Nat Commun. 2020;11:5892.
- 24. Yang X, Wang A, Qiao B, Li J, Liu J, Zhang T. Single-atom catalysts: a new frontier in heterogeneous catalysis. Acc Chem Res. 2013;46:1740–8.
- Hou L, Tian C, Yan Y, Zhang L, Zhang H, Zhang Z. Manganese-based nanoactivator optimizes cancer immunotherapy via enhancing innate immunity. ACS Nano. 2020;14:3927–40.
- Katz N, Rader DJ. Manganese homeostasis: from rare single-gene disorders to complex phenotypes and diseases. J Clin Investig. 2019;129:5082–5.
- Li L, Yang X. The essential element manganese, oxidative stress, and metabolic diseases: links and interactions. Oxid Med Cell Longev. 2018;2018:7580707.
- Lv M, Chen M, Zhang R, Zhang W, Wang C, Zhang Y, et al. Manganese is critical for antitumor immune responses via cGAS-STING and improves the efficacy of clinical immunotherapy. Cell Res. 2020;30:966–79.
- Pei J, Dou H, Liu C, Li T. Manganese single-atom nanostructures for highly efficient tumor therapy. J Ind Eng Chem. 2022;109:330–7.
- Zhu Y, Wang W, Cheng J, Qu Y, Dai Y, Liu M, et al. Stimuli-responsive manganese single-atom nanozyme for tumor therapy via integrated cascade reactions. Angew Chem Int Ed. 2021;60:9480–8.

- Fang J, Islam W, Maeda H. Exploiting the dynamics of the EPR effect and strategies to improve the therapeutic effects of nanomedicines by using EPR effect enhancers. Adv Drug Del Rev. 2020;157:142–60.
- Zi Y, Yang K, He J, Wu Z, Liu J, Zhang W. Strategies to enhance drug delivery to solid tumors by harnessing the EPR effects and alternative targeting mechanisms. Adv Drug Del Rev. 2022;188:114449.
- Ye J, Lv W, Li C, Liu S, Yang X, Zhang J, et al. Tumor response and NIR-II photonic thermal co-enhanced catalytic therapy based on single-atom manganese nanozyme. Adv Funct Mater. 2022;32:2206157.
- Feng J, Gao H, Zheng L, Chen Z, Zeng S, Jiang C, et al. A Mn-N3 singleatom catalyst embedded in graphitic carbon nitride for efficient CO₂ electroreduction. Nat Commun. 2020;11:4341.
- 35. Li W, Li T, Wey M. Preferred enhancement of fast-SCR by Mn/CeSiOx catalyst: study on Ce/Si promotion and shape dependence. Chem Eng J. 2021;403:126317.
- Wang Y, Cho A, Jia G, Cui X, Shin J, Nam I, et al. Tuning local coordination environments of manganese single-atom nanozymes with multi-enzyme properties for selective colorimetric biosensing. Angew Chem Int Ed. 2023;62:e202300119.
- Liu Y, Wei Z, Zhong B, Wang H, Xia L, Zhang T, et al. O-, N-coordinated single Mn atoms accelerating polysulfides transformation in lithium-sulfur batteries. Energy Stor Mater. 2021;35:12–8.
- Guo Z, Xie Y, Xiao J, Zhao Z, Wang Y, Xu Z, et al. Single-atom Mn–N₄ site-catalyzed peroxone reaction for the efficient production of hydroxyl radicals in an acidic solution. J Am Chem Soc. 2019;141:12005–10.
- Hui K, Fu J, Liu J, Chen Y, Gao X, Gao T, et al. Yolk–shell nanoarchitecture for stabilizing a Ce2S3 anode. Carbon Energy. 2021;3:709–20.
- Ahmed Y, Zhong J, Wang Z, Wang L, Yuan Z, Guo J. Simultaneous removal of antibiotic resistant bacteria, antibiotic resistance genes, and micropollutants by FeS₂@GO-based heterogeneous photo-Fenton process. Environ Sci Technol. 2022;56:15156–66.
- Dong S, Dong Y, Jia T, Liu S, Liu J, Yang D, et al. GSH-depleted nanozymes with hyperthermia-enhanced dual enzyme-mimic activities for tumor nanocatalytic therapy. Adv Mater. 2020;32:2002439.
- 42. Jiang B, Duan D, Gao L, Zhou M, Fan K, Tang Y, et al. Standardized assays for determining the catalytic activity and kinetics of peroxidase-like nanozymes. Nat Protoc. 2018;13:1506–20.
- Gao L, Zhuang J, Nie L, Zhang J, Zhang Y, Gu N, et al. Intrinsic peroxidase-like activity of ferromagnetic nanoparticles. Nat Nanotechnol. 2007;2:577–83.
- Calle P, Fernández Arizpe A, Sieiro C. Photosensitization by harmine: an ESR spin trapping study on the generation of the superoxide anion radical. Appl Spectrosc. 1996;50:1446–51.
- Moan J, Wold E. Detection of singlet oxygen production by ESR. Nature. 1979;279:450–1.
- Du F, Liu L, Wu Z, Zhao Z, Geng W, Zhu B, et al. Pd-single-atom coordinated biocatalysts for Chem-/Sono-/Photo-Trimodal tumor therapies. Adv Mater. 2021;33:2101095.
- Wang C, Cao F, Ruan Y, Jia X, Zhen W, Jiang X. Specific generation of singlet oxygen through the Russell mechanism in hypoxic tumors and GSH depletion by cu-TCPP nanosheets for cancer therapy. Angew Chem Int Ed. 2019;58:9846–50.
- 48. Niu B, Liao K, Zhou Y, Wen T, Quan G, Pan X, et al. Application of glutathione depletion in cancer therapy: enhanced ROS-based therapy, ferroptosis, and chemotherapy. Biomaterials. 2021;277:121110.
- Li J, Wang J, Zhang J, Han T, Hu X, Lee MMS, et al. A facile strategy of boosting photothermal conversion efficiency through state transformation for cancer therapy. Adv Mater. 2021;33:2105999.
- Paściak A, Pilch-Wróbel A, Marciniak Ł, Schuck PJ, Bednarkiewicz A. Standardization of methodology of light-to-heat conversion efficiency determination for colloidal nanoheaters. ACS Appl Mater Interfaces. 2021;13:44556–67.

Publisher's Note

Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.